

09/889908

Attny Docket No. B1180/20003
PTO Customer No. 03000

**TRANSMITTAL LETTER TO THE UNITED STATES
DESIGNATED/ELECTED OFFICE (DO/EO/US)
CONCERNING A FILING UNDER 35 U.S.C. 371**

(ENTRY INTO U.S. NATIONAL PHASE UNDER CHAPTER II)

International Application No. : PCT/EP00/00621

International Filing Date : January 26, 2000

Priority Date Claimed : January 26, 1999 (DE 19903001.4)

Title of Invention : PROCESS AND DEVICE FOR THE DETECTION
OF MICROSCOPICALLY SMALL OBJECTS

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Box PCT (EO/US)
Commissioner for Patents
Washington, D.C. 20231

Sir:

Applicant herewith submits to the United States Designated/Elected Office (DO/EO/US) the following items and other information:

1. This is a **FIRST** submission of items concerning a filing under 35 U.S.C. 371.
2. This is an express request to immediately begin national examination procedures (35 U.S.C. 371(f)).
3. A proper Demand for International Preliminary Examination was made by the 19th month from the earliest claimed priority date.
4. A copy of the International Application as filed (35 U.S.C 371(c)(2)) has been transmitted by the International Bureau. A copy of the cover sheet of the international application as published on August 3, 2000, under International Publication No. WO 00/45147 is attached hereto.
5. An English translation of PCT Application No. PCT/EP00/00621, as filed, is enclosed.
6. A Preliminary Amendment is enclosed.
7. An Abstract of the Disclosure is attached to the Preliminary Amendment.
8. An Information Disclosure Statement and attached references are enclosed.
9. Calculation sheet, in duplicate, is attached.

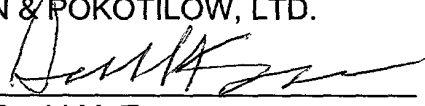
This application and items attached are being transmitted before the 30 month claimed priority date.

Respectfully submitted,

CAESAR, RIVISE, BERNSTEIN,
COHEN & POKOTILOW, LTD.

July 24, 2001

By


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JC17 Rec'd PCT/PTO 24 JUL 2001

CALCULATION SHEET
BASIC NATIONAL FEE (37 CFR 1.492(1)(1)-(5)):

Claims Fee

	Claims Filed	Extra Claims	Rate	Calculation
Total Claims	22	2	x 18	\$36.00
Independent Claims	3	0	x 80	
Multiple Dependent Claims			x270	

Basic Fee U.S. PTO was not International Preliminary Examination Authority. Search report on the international application was prepared by the European Patent Office
 Total

\$ 860.00
 \$ 896.00

Reduction by ½ for filing by small entity

TOTAL NATIONAL FEE **\$ 896.00**

Please charge counsel's account no. 03-0075 in the amount of \$896, or any additional amount which may be required, to cover the above fees. Duplicate copies of the calculation sheets are enclosed.


AUTHORIZATION TO CHARGE ADDITIONAL FEES

The Commissioner is hereby authorized to charge the following additional fees which may be required by this paper and during the entire pendency of this application to counsel's deposit account:

1. 37 CFR 1.492(a)(1), (2), (3) and (4) (filing fees)
2. 37 CFR 1.492(b), (c) and (d) (presentation of extra claims)
3. 37 CFR 1.17 (application processing fees)
4. 37 CFR 1.492(e) and (f) (surcharge fee for filing declaration and/or filing an English translation of an International Application later than 30 months after the priority date)

03-0075
 Deposit Account

July 24, 2001
 Date


 David M. Tener, Reg. No. 37,054

09/889908

IN THE UNITED STATES PATENT AND TRADEMARK OFFICE
PATENT EXAMINING OPERATION

Applicant(s): Günter FUHR et al.

Serial No: U.S. national stage application based on
PCT/EP00/00621, filed January 26, 2000

Filed: Examiner:

Att. Docket No.: B1180/20003 Confirmation No.:

For: PROCESS AND DEVICE FOR THE DETECTION OF MICROSCOPICALLY
SMALL OBJECTS

PRELIMINARY AMENDMENT

Box PCT
Commissioner for Patents
Washington, D.C. 20231

Attention: DO/EO/US

Sir:

Please amend the above-identified application as follows:

IN THE CLAIMS:

Please cancel claims 1-21 without prejudice or disclaimer, and
add the following new claims:

22. A process for object detection, comprising the steps:
enlarged optical imaging of at least one resting or moving
object on a structured mask with at least one segment
adapted for transmitting light from a flat section to a
detector unit, wherein said object is located at least
partially or temporarily in said flat section, and said
flat section has a characteristic dimension smaller than
a dimension of the object or a movement path of the
object;

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detecting a quantity of light transmitted by the structured mask;

generating a detector signal having a predetermined relationship with the quantity of light; and

evaluating the detector signal in regard to at least one of a presence of the object, a position of the object, a shape of the object, and a temporal change of the position of the object.

23. The process according to claim 22, wherein the object comprises synthetic or biological particles in a microchannel of a fluidic microsystem, wherein the particles are subjected to at least one of hydrodynamic, acoustic, magnetic and electrical forces.

24. The process according to claim 23, wherein the structured mask is positioned in relation to the fluidic microsystem in such a way that light is transmitted by the structured mask from a section in which the particles are to be positioned or moved.

25. The process according to claim 23, wherein the structured mask is positioned in relation to the fluidic microsystem in such a way that light is transmitted by the structured mask from a section into which the particles are not to enter.

26. The process according to claim 22, further comprising at least one of the following additional steps:

detecting a presence of a resting particle by detecting whether the detector signal has a predetermined, unchanging amplitude;

detecting a presence of a moving particle at a specific position by determining whether the detector signal has a predetermined time characteristic;

detecting frequencies and speeds of particles by evaluating maxima of the detector signal in regard to width and interval of the maxima; and

counting particles by counting the maxima of the detector signal.

27. The process according to claim 26, further comprising at least one of determining a direction of particle movement, and size-dependent counting of particles.

28. The process according to claim 22, further comprising at least one of evaluating an amplitude of the detector signal, and evaluating a variability of the detector signal.

29. The process according to claim 23, wherein the particles are fixed or moved with a trapping laser.

30. The process according to claim 29, wherein the particles are brought into contact with a modification layer, a cell, or receptors in the fluidic microsystem with the trapping laser and, during the evaluation of the detector signal in regard to movement characteristics of the particles, parameters are determined which

are characteristic for interaction of the particles with the modification layer, the cell, or the receptors.

31. A device for object detection, which comprises:

an optical imaging unit for enlarged imaging of at least one resting or moving object on a structured mask, having at least one light transmitting segment adapted to transmit light from a flat section to a detector unit, wherein the object is located at least partially or temporarily in the flat section and the flat section has a characteristic dimension smaller than a dimension of the object or a movement path of the object;

a detector unit for detecting a quantity of light transmitted by the structured mask and for forming a detector signal having a predetermined relationship with the quantity of light; and

an evaluation unit for evaluation of the detector signal in regard to at least one of a presence of the object, a position of the object, a shape of the object and a temporal change of the position.

32. The device according to claim 31, wherein the optical imaging unit is part of a microscope.

33. The device according to claim 32, wherein the structured mask is positioned in a beam path of the microscope.

34. The device according to 31, wherein the structured mask

35. The device according to claim 34, wherein multiple

36. The device according to claim 34, wherein at least one

37. The device according to claim 31, wherein the detector

38. The device according to claim 31, adapted for object

39. The device according to claim 38, wherein the particles

40. The device according to claim 38, wherein a trapping

41. The device according to claim 31, wherein the light

the object or a movement path of the object, or is smaller than an image of the object or a movement path of the image.

42. The process of claim 22, further comprising at least one of: (a) dielectric single particle spectroscopy in fluidic microsystems; (b) measurement of electromagnetic forces in microelectrode arrangements; (c) measurement of optical forces in trapping lasers; (d) detection of the function of microelectrodes in microsystems; (e) detection of at least one of particle positions, particle movements, particle numbers, and particle interactions; and (f) measurement of particle rotations induced by rotating electrical fields.

43. A process for object detection, with the steps:
optical imaging of at least one resting or moving object on a
CCD matrix detector;
electronic masking of a signal of said CCD matrix detector for
providing signals from specific image points of said
object; and
evaluating said signals from specific image points in regard
to at least one of a presence of the object, a position
of the object, a shape of the object and a temporal
change of the position.

IN THE ABSTRACT

Please enter the attached abstract in the application.

REMARKS

Claims 1-21 have been replaced by Claims 22-43, to eliminate multiple-dependency from the claims, and to conform the claims to U.S. practice. Applicants respectfully submit that the claims are supported by the application as originally filed as a PCT application.

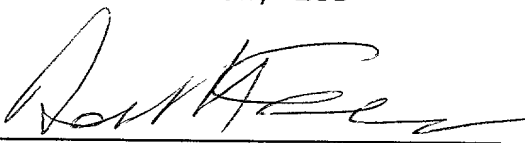
The Abstract of the Disclosure is also attached hereto to comply with the requirements of 37 C.F.R. §1.72(b).

Prompt and favorable consideration is respectfully requested.

Should the Examiner believe that anything further is desirable in order to place the application in even better condition for initial examination and allowance, the Examiner is invited to contact Applicants' undersigned attorney at the telephone number listed below.

Respectfully submitted,

CAESAR, RIVISE, BERNSTEIN,
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July 24, 2001

Please charge or credit our Account No. 03-0075 as necessary to effect entry and/or ensure entry and/or consideration of this submission.

ABSTRACT OF THE DISCLOSURE

For object detection, particularly in fluidic microsystems, optical imaging of at least one resting or moving object (10) on a structured mask (20) with at least one segment from a flat section (80), in which the object (10) is located at least partially or temporarily and which has a characteristic dimension smaller than the dimension of the object (10) or its movement path, to a detector unit, detection of the quantity of light transmitted by the structured mask (20), and generation of a detector signal which has a predetermined relationship with the quantity of light, and evaluation of the detector signal in regard to the presence of the object (10), its position, its shape and/or the temporal change of the position are performed.

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PROCESS AND DEVICE FOR THE DETECTION OF MICROSCOPICALLY
SMALL OBJECTS

The invention concerns a process and a device for the detection of microscopically small objects, particularly for the detection of the presence and/or for the measurement of the location and/or the change in location of the objects, for example in fluidic microsystems. The microscopically small objects are particularly synthetic or biological particles which are manipulated in a fluidic microsystem. The invention also concerns uses of the process and/or the device, particularly for object detection depending on mechanical, electrical, or chemical interactions of the objects with their environment or other objects.

Using fluidic microsystems for particle-specific manipulation of microscopically small objects under the effect of hydrodynamic and/or electrical forces is generally known. The manipulation of biological particles in microsystems with high frequency electric fields on the basis of negative dielectrophoresis is, for example, described by G. Fuhr et al. in "Naturwissenschaften", vol. 81, 1994, p. 528 et seq.. The manipulation of the objects comprises, among other things, sorting according to specific characteristics, alteration of the object under the effect of electrical fields (e.g. cell poration), chemical treatment, mutual bringing together and interaction of the objects and similar actions. The provision of predetermined hydrodynamic and/or electrical forces is performed through the design of the channel structure of the microsystem and/or the geometric shapes of microelectrodes for forming high frequency electric fields and their control.

The previously known microsystems do allow monitoring of the object manipulation occurring with optical means, e.g.

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using a microscope with a camera. This optical monitoring has, however, been restricted until now to visual examinations or the use of costly image recognition processes for processing the camera image. The image processing processes are, however, significantly too slow for the object speeds which arise, if real-time monitoring is to be practiced. Therefore, until now the implementation of automatic system controls, in which, for example, specific process variations occur depending on location, movement state, or number of objects observed, has been excluded.

A process for movement detection of microscopic objects which perform an at least partially periodic movement is known from PCT/EP97/07218. This process is based on the use of a Fourier analysis of a detector signal which characterizes the object movement over multiple movement periods. This process represents a significant simplification relative to the use of computer-aided image processing processes, but it is restricted to applications with periodic movements. In general, however, non-periodic movements or rest conditions of the objects also occur in a microsystem, the detection of which, particularly for automatic control of a microsystem, is also of interest.

Detecting the presence of small particles in suspensions on the basis of scattered light measurements is also known. However, this principle can only be realized with multiple particles, and can therefore not be particle-specific. In addition, no information on the movement state of particles (location, speed, or similar parameters) can be derived.

It is the object of the invention to indicate an improved process for object detection which can be used in any desired movement or rest state of the objects to be detected and which allows rapid and reliable signal evaluation. The object of the invention is also to indicate devices for im-

plementing such a process and new applications of the object detection according to the invention.

These objects are achieved by a process and device with features according to the claims 1 and 10, respectively. Advantageous embodiments and applications of the invention arise from the dependent claims.

The invention is based on the idea of imaging the locational area (movement path or position) of the object to be detected enlarged on a mask which is set up in at least one segment for transmitting (reflection or transmission) of the light from one part of the locational area (so-called section) and otherwise for suppressing of transmission outside the segment. The at least one light-transmitting segment of the mask has a characteristic dimension which is smaller than the image of the entire object or the lateral extension of the movement path of the object. The quantities of light of the object image transmitted by the mask are summarily imaged on a detector device, at which a detector signal is generated having a predetermined relationship with the quantity of light detected and allowing an evaluation in regard to the presence of the object, its position, and/or the temporal change of the position. The quantity of light detected by the detector device is modulated in a characteristic way by the masked image of a section of the object and/or of the object path. The time dependence of the detector signal, particularly the temporal position of signal maxima, the amplitudes of the signal maxima, and the temporal amplitude shape in the vicinity of the signal maxima provides information not only on the location and the speed of the objects, but also on derived dimensions such as the frequency of periodic movements, quantitative information on particle numbers, movement direction, centering in the microsystems, or similar dimensions.

One subject of the invention is therefore particularly object detection on the basis of a diaphragma measurement principle, in which a summary detection of the quantities of light coming out of a section of the object or the object path occurs. Correspondingly, the partial object imaging can, in principle, occur on a diaphragma (screen) with suitable dimension. In the simplest case, the mask consists of an element opaque to light with a round or angular opening which is suitably dimensioned for realization of the partial image of the object to be detected according to the invention.

However, corresponding to preferred embodiments of the invention, the mask has a segmentation with a predetermined geometry. The at least one segment for transmission of the light of the partial image has a geometric shape which is selected, depending on the application, according to the respective object movements (e.g. translation, rotation, translational vibration, rotational vibration, or similar movements) expected at the measurement point.

According to the invention, an enlarged image of the locational area of the objects to be detected (e.g. in a microsystem) is preferably provided on the mask. For this purpose, the segmentation of the mask, which is set up for transmission of the light from a partial image, can be absolutely larger than the section or part of the object concerned. This is advantageous for the production and justification of the mask.

Preferred applications of object detection according to the invention are provided in fluidic microsystems, particularly in automatic regulation of system functions, in dielectric single particle spectroscopy, and in the examination of interactions between objects and other objects and/or substrates. Objects detected according to the invention have a characteristic diameter in the range below 500

µm down to the 100 nm range and comprise synthetic or biological particles (or particle aggregates). The synthetic particles are, for example, membrane-enclosed formations, such as liposomes or vesicles, or plastic particles (so-called beads). The biological particles are biological cells or cell aggregates or cell components, microorganisms, viruses, or similar objects.

One subject of the invention is also a device for implementation of object detection according to the invention, comprising an optical imaging unit for imaging a part of an object to be detected (or of its path) via a mask on a detector unit, which generates a detector signal in a specific relationship with the quantity of light detected, and an evaluation unit for determining characteristics of the movement or rest state of the object. The imaging unit contains, in particular, the mask, on which the object or its movement path is imaged in enlarged form and which only transmits a section of the image to the detector unit. According to a preferred embodiment of the invention, which is explained in detail below, the mask is a screen with a predetermined transmission geometry. The invention is, however, not restricted to this design, but can also be implemented with other mask designs which are set up to fulfill the same function as the transmitting screen. Instead of a transparent segment in an opaque mask material, an opaque segment (with the same geometry as the previously mentioned transparent segment) can be used as the mask in an otherwise transparent environment. Correspondingly, a reflection principle can be realized instead of the transmission principle.

The imaging unit is preferably part of a microscope arrangement, which is known per se, containing the mask for generating the partial image in the beam path. In this way, visual object observation can occur simultaneously with object detection. The combination with the microscope ar-

rangement is, however, not urgently necessary. Particularly for automatic applications, the imaging unit can be provided directly in a microsystem.

The invention has the following advantages. The object detection according to the invention does not require imaging processing processes which are costly in measurement and time. It allows highly precise measurement with imaging and measurement units which are available per se. An existing microscope assembly can be set up for object detection according to the invention simply by attaching the mask mentioned. The mask segmentation according to the invention allows object detection without a large amount of adjustment. The object detection can be automated easily. Particular advantages result in the combination of mask-based detection with dielectric single particle spectroscopy for highly precise determination of dielectric particle characteristics from the movement characteristics of the particles in high frequency electric fields. Through the use of predetermined mask types, a device according to the invention can be adjusted without problems for the detection of greatly varying types of movement, without having to resort to image processing methods or having to perform a modification of the system. It is sufficient for a detector unit to contain one single detector whose measurement signals can be serially processed. This allows processing in real time, which is particularly significant for switching and sorting applications in microsystems.

A further advantage of the invention arises from the geometric mask structuring. In contrast to the typical "pin-hole" measurement principle, the mask segments are designed as smaller than the image of the entire object, but, unlike apertures (as they are known in, for example, confocal microscopy), are implemented as planar. In this way, increased functional reliability is achieved, even with deviations of the objects from the expected movement paths

which occur in practice. The mask segmentation allows for compensation of tolerances as the object moves.

Further characteristics and advantages of the invention are described in the following with reference to the attached drawings. These show:

- Figs. 1A, 1B a schematic perspective view of a micro-electrode arrangement for illustration of the detection principle according to the invention in the example of a first mask shape,
- Figs. 2 to 12, schematic top views of microelectrode arrangements for illustration of further mask shapes, with characteristic traces of the detector signals being illustrated in the lower part of the figures,
- Figs. 13A, 13B to 15 schematic perspective views of micro-electrode arrangements for illustration of the investigation of interactions between a test object and a substrate or another object,
- Figs. 16 to 18 schematic perspective views of microelectrode arrangements for illustration of a force or field measurement in the microsystem, and
- Fig. 19 a block diagram of an exemplary embodiment of the detector unit according to the invention.

The invention will be described in the following with the example of fluidic microsystems for the manipulation of synthetic or biological particles. The realization of the

invention is not bound to specific particle types. However, it is necessary for specific applications that the particles have a surface structure which can be imaged (e.g. structures on biological cells). If this is not initially present, however, the particles can also be provided with structuring (e.g. with a fluorescence marking). The microsystems have a channel structure with typical transverse dimensions in the μm range and typical lengthwise dimensions in the mm range. Microelectrodes having predetermined electrode shapes and arrangements, which are set up to have high frequency voltages (frequencies in the kHz to MHz range, amplitudes in the mV to V range) applied to them in order to subject the particles flowing or resting in a suspension in the channels to electric fields, are affixed to the channel walls. Under the effect of the electric fields, a predetermined force is exercised on the particles on the basis of negative or positive dielectrophoresis. Further particulars of these fluidic microsystems are known per se and are therefore not described in the following. Furthermore, it is to be emphasized that the invention is not restricted to fluidic microsystems, but can also be realized in other applications in which individual objects, particularly microscopically small objects, are to be detected, specifically in regard to their presence, their position, and their speed.

Fig. 1A shows a schematic perspective view of a section of a microsystem with a channel 50, with only the channel bottom 51 and the channel cover 52 illustrated, which, for example, can have a particle suspension flow through it (from the front to the rear in the illustration). The electrode arrangement 40 is an octopole arrangement, with four microelectrodes 41 on the channel bottom 51 and four microelectrodes 42 on the channel cover 52. A rotating electrical field (rotational field) is generated with the electrode arrangement 40 in a way a which is known per se, with the particle 10 being held in its center in the focus 61 of a

trapping laser 60. The trapping laser 60 is part of a so-called optical tweezer (or laser tweezer), as it is known per se.

At least one wall of the channel 50 (e.g. the channel cover 52) is optically transparent. An imaging unit according to the invention is provided, on the side of the transparent channel wall having a thickness less than or equal to 250 μm , which is intended for imaging a section 80 of the locational area of the particle 10 (in this case the center of the electrode arrangement 40) on a detector unit. The essential element of the imaging unit, which is otherwise not illustrated, is the mask 20 in the form of an essentially flat screen with a predetermined geometric transmission shape. In the example illustrated, the transmission shape is in the form of crossing strips. The strips form the segments 30 of the mask 20. In general, the segments of the mask according to the invention are preferably positioned flat or two-dimensionally in order to obtain the information on the location of the particles and/or the changes in location.

The locational area of the particle 10, and therefore also the section 80 and/or a part of the section 10, are imaged with optical elements (not shown) on the plane of the mask 20. The mask 20 transmits a part of the light forming the image of the particle 10 to the detector (also not shown). If the location of the particle 10 in the microsystem changes, the light summarily captured at the detector by the mask 20 will be modulated in correspondence with the particle structures currently imaged on the mask plane. The particle structures comprise, for example, lighter and darker regions of the particle image. During movement of the particle, the mask 20, which is fixed relative to the microsystem, transmits a larger or smaller quantity of light to the detector depending on the image brightness imaged on the segments.

The image of the particle on the mask plane is an enlarged image. The enlargement factor is selected depending on the application and is, for example, approximately 10 to 20, e.g. 15, in microsystem - microscope combinations. Characteristic dimensions of the segments 30 of the mask are in the range of approximately 100 μm (strip length).

A corresponding arrangement is illustrated in top view in Fig. 1B. For dielectric single particle spectroscopy, the rotation of the particle 10 is to be detected depending on the amplitude and/or frequency of the rotational field. Information on the dielectric characteristics of the particle 10 can be determined from its angular velocity. The rotational field can rotate continuously or (as shown) have a running direction change, so that vibrations in the particle states 11a, 11b on both sides of a central position result. The section 80 covered with the cross corresponding to the mask shape is imaged via the mask. The light transmitted by the mask is modulated according to the vibrations mentioned. The vibration frequency can thus be inferred directly from the detector signal and supplied for evaluation.

Fig. 2 illustrates an application of the invention with a modified mask design. It is emphasized that the masks are not illustrated in each of the illustrations of the figures 2 to 12. In any case, each of the sections of the locational area of the particles to be detected, from which light is transmitted by the mask, are indicated. The corresponding mask segments have the same geometric shape, but are implemented larger than the sections shown due to the enlarged image introduced. The mask is structured in such a way that the light from the section 80 of the microsystem with or without the particle 10 is transmitted to the detector unit.

The design according to Fig. 2 serves for object detection for measuring dielectrophoretic characteristics of the particle 10. The particle 10 is inside a microelectrode arrangement 40, with only the electrodes 41 on the channel bottom 51 shown schematically. This electrode arrangement can in turn have four electrodes added on the channel cover to become an octopole. Other multiple electrode arrangements are also possible. At frequencies of the electrode voltages, which are selected depending on the application, the particle 10 is moved at various speeds by repulsion and/or attraction between the electrodes, depending on the external conductivity and the dielectric particle characteristics. This movement occurs periodically, for example. The particle runs, depending on its vibrational frequency, along the directions indicated with arrows (or in other directions as well) through the section 80, which corresponds exactly with the transmission geometry of the mask. The detector signal (arbitrary units) is thus modulated depending on frequency, as is indicated in the lower part of Fig. 2. The signal trace D1 corresponds to a specific frequency and a slow movement of the particle 10 between the electrodes 41. The signal trace D2 shows the same frequency, but a smaller width of the maxima of the detector signal. This corresponds to an increased movement speed of the particle 10 (and an increased displacement).

Fig. 3 illustrates a further mask design in which the mask consists of four separate quadrilateral segments positioned in such a way that the sections 80a to 80d are imaged on these segments. In this way, the period the particle 10 stays at the electrodes 41 during periodic movement can be measured (analogous to Fig. 2). The segments each serve as partial masks for object detection. The detector signal determined by the detector summarily comprises all of the quantities of light transmitted from all segments. In turn, long periods of stay (D1) can be differentiated from short periods of stay (D2) according to the lower part of Fig. 3.

Fig. 4 illustrates object detection for the detection of the slightest thermal or hydrodynamic vibrations of a particle 10 between the electrodes 41. The mask has a grid-shaped segment arrangement, so that the light from the section 80 in the microsystem is transmitted to the detector. The lower part of Fig. 4 illustrates the possibility of differentiation of stronger particle vibrations, which lead to high frequency noises D1, from smaller vibrations with a lower noise frequency (trace D2).

Fig. 5 illustrates an embodiment of the invention in which the presence of particles in an arrangement of electrodes in a row is investigated. The electrode arrangement 40 in this case consists of electrode bands 43 which are shaped like a triangular function. In Fig. 5, again only the electrode bands 43 on the channel bottom 51 are shown. The direction of flow in the channel is indicated by the arrow. The electrode bands 43 are driven in such a way that they form field minima at periodic intervals in which the particles 10a to 10d are to be positioned.

The mask consists of a group of segments whose number corresponds to the number of field minima of the electrode arrangement 40. Each segment forms a square frame. The segments of the mask are positioned in such a way that light from the sections 80a to 80d of the microsystem is imaged on the detector via the mask. Depending on the illumination conditions, a specific contribution to the summary detector signal results, upon the presence of a particle in a field minimum, which can assume four predetermined amplitudes in the sequence of four particles 10 illustrated. If, for example, the sequential electrode arrangement is completely filled with particles, the maximum amplitude is reached, which is illustrated in trace D1 with the solid line. In contrast, if all field minima are free of particles, the lowest amplitude results, which is shown in trace D1 with

dots. As an alternative to detection of the amplitude of the detector signal, oscillations of the amplitude can also be measured. This is illustrated with the trace D2. Correspondingly, information on the stability of the particles in the sequential electrode arrangement can be inferred from this so-called variance effect.

A modified mask design for examining the particle sequence is illustrated in Fig. 6. The mask consists of strip-shaped segments at intervals from one another which image the sections 80a to 80h of the microsystem on the detector. The segment strips have alternating varying lengths and are positioned in such a way that the longer segment strips detect the sections 80a, 80c, 80e, and 80g corresponding to the field minima between the electrode bands 43 and the shorter segment strips detect the sections 80b, 80d, 80f, and 80h of the microsystem. The detector signal has, in turn, a trace which essentially corresponds to the illustration in the lower part of Fig. 5, with, however, additional amplitude steps corresponding to the particle detection occurring at the locations between the field minima.

Fig. 7 illustrates the principle of the detection of the movement direction according to the invention. The upper part of Fig. 7 is a schematic top view of a channel in which the channel side walls 53, 54 adjoining the channel bottom 51 are also illustrated. The mask has a T-shaped transmission geometry and is formed by two straight strip-shaped segments, with one longer segment aligned in the lengthwise channel direction (corresponding to the direction of the arrows) and a shorter segment strip running perpendicular to this at the end of the longer segment strip. The image on the mask leads to transmission of the light from the T-shaped section 80 of the microsystem to the detector.

The detector signal then has one of the traces illustrated in the lower part of Fig. 7, depending on the movement direction. The particle 10a, which moves from left to right, contributes first at the lengthwise strip 80a and then at the transverse strip 80b to the detector signal, which, corresponding to the trace D1, first slowly increases as the particle passes through and then quickly drops after the particle 10a passes the transverse strip 80b. For the particle 10b, which moves from right to left, the reverse relationships result. The detector signal first increases quickly and then drops slowly, corresponding to the trace D2. The detector signal thus has a characteristic time characteristic which provides information on the movement direction of the particle in the channel.

A mask according to the invention can also be designed in such a way that differences in shape of particles in the microsystem can be detected. This is illustrated in Fig. 8, which again shows a top view of the channel with the channel bottom 51 and the channel side walls 53, 54. Particles 10a, 10b, and 10c, which have various geometries, move in the channel.

The mask consists of two strip-shaped segments which are each curved into a semicircle and which touch at their apexes. In this way, the mask allows the transmission of the light coming out of the section 80 of the microsystem to the detector. Depending on the time characteristic of the detector signal, the respective particles passing by the section 80 can be distinguished. This is illustrated in the lower part of Fig. 8.

The oblong particle 10a generates a signal trace D1 because the detector signal is modulated for a relatively long time, but only has a relatively low amplitude due to the small transverse extension of the particle 10a. For a round particle 10b, to whose shape the semicircular curvature of

the mask segments is tailored, the trace D2 results. The entrance of the particle 10b into the section 80 causes a rapid signal increase. A corresponding situation applies for the case when the particle 10b leaves the section 80. Finally, the particle 10c (pair) leads to the signal trace D3, which extends over a larger time range than particle 10b due to the greater lengthwise extension and reaches a higher amplitude than particle 10a due to the larger transverse extension.

The mask shape described above with reference to Fig. 2 can also be used for particle counting, as is illustrated in Fig. 9. The mask contains two segments which are set up for transmission of light from the sections 80a, 80b and which each have the shape of a square frame. The sections 80a, 80b are positioned in the lengthwise channel direction at a predetermined interval. The selection of the interval and the size of the sections 80a, 80b (and/or the corresponding mask segments) is selected depending on the particle sizes occurring and the flow speed in the channel. The particle counting can even be performed size-selectively.

Thus, the smallest particle 10a produces the signal trace D1 with two separate maxima corresponding to the passage of the particle 10a at each of the sections 80a, 80b. For the medium particle 10b, the signal trace D2 results, in which the maxima run into one another. For a sufficiently large particle 10c with a characteristic size which is comparable with the interval of the sections 80a, 80b the signal trace D3 with one single maximum results. The signal traces D1 and D2 can additionally be used to determine the particle speed from the interval of the maxima.

Fig. 10 again shows a top view of the channel with the channel floor 51 and the channel side walls 53, 54. In the channel, particles 10a, 10b move with the flowing suspension fluid according to the direction of the arrow. The ob-

ject detection according to the invention is designed here in such a way that it is determined whether a particle moves in the center of the channel or more at the edge of the microchannel. For this purpose, the mask has two segments made of straight, crossing strips which are positioned in such a way that the light from the sections 80a, 80b of the microsystem is transmitted to the detector. The sections 80a, 80b each extend as straight strips over the entire width of the channel and are curved relative to the transverse channel direction, so that an X-shape with the strips intersecting in the center of the channel results.

Detection through a mask which transmits the light from sections 80a, 80b selected in this way results in a signal trace D1 with one single maximum if the particle 10b moves in the center of the channel or a signal trace D2 if the particle 10a moves at the edge of the channel, so that each section 80a, 80b is crossed two times.

A similar monitoring function is illustrated in Fig. 11, which depicts a top view of a channel with focusing electrodes 44 on the channel bottom 51. The focusing electrodes 44 form field barriers, which the particles 10a cannot penetrate, when high frequency voltages are applied to them, so that, in combination with the force of the flow, a particle movement toward the center of the channel occurs. If one of the focusing electrodes 44 fails, particles 10b can pass by the electrodes except at the center.

In order to detect this type of malfunction of the focusing electrodes 44, the mask is designed in such a way that particles at the channel edge can again be distinguished from particles in the center of the channel. For this purpose, the mask has three segments, comprising two straight strip-shaped segments and one dot-shaped segment, which are positioned in a straight row transverse to the lengthwise channel direction. The segments are set up for the purpose of

transmitting the light from the sections 80a, 80b, and 80c of the microsystem to the detector. After the passage of each of the particles 10a through the center or the particles 10b through the edges of the channel, the signal traces shown in the lower part of Fig. 11 result. The signal trace D1 shows a high amplitude, i.e. a strong modulation of the detector signal. This indicates the particle 10b has passed through the sections 80a or 80c and therefore one or both of the focusing electrodes 44 is switched off or defective. In contrast, the signal trace D2 shows a small modulation corresponding to particle passage through the center of the channel. The signal corresponding to the signal trace D2 can in turn be used as the count signal for counting the particles 10b which have passed the focusing arrangement.

A mask such as that described with reference to Fig. 2 can also be used for checking the function of a deflection electrode 45. This application of the invention is illustrated in Fig. 12. The deflection electrode 45 is a micro-electrode on the channel bottom 51 in the shape of a curved electrode strip. The deflection electrode 45, in combination with a corresponding deflection electrode (not shown) on the channel cover, forms a curved field barrier, when high frequency voltages are applied to it, which the flowing particles 10a and/or 10b can pass at various distances from the channel side walls 53, depending on their dielectric characteristics. If the deflection electrode 45 is switched on, the smallest particles 10a, in which the smallest polarization forces are induced, can pass the field barrier even at the edge of the channel, while the larger particles 10b run further toward the center of the channel until the force of the flow is sufficiently large that passage of the field barriers is effected. If the deflection electrode 45 is switched off, both large and small particles can flow further at the channel edge.

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The mask has a square, frame-shaped segment which is set up for the purpose of transmitting the light coming out of the section 80 of the microsystem to the detector. If only small particles 10a pass by the section 80, then the signal trace D1 with two separate maxima occurs, corresponding to the passage of the small particles 10a at the two frame sides in the direction of flow. If the deflection electrode 45 is switched off or defective, then larger particles are also detected via the mask, so that the signal trace D2 occurs, with one single, widened maximum.

The above exemplary embodiments described with reference to Figs. 1 to 12 relate to particle detection in microsystems, known per se, with channel structures made of materials which are inert relative to the particles. The figs. 13 to 15 described below show a particularly advantageous application of the invention in modified microsystems in which the interaction of the particles with the channel walls is not avoided, but encouraged in predetermined ways. This modification is illustrated in figs. 13A and 13B in analogy to the illustration according to Fig. 1.

Fig. 13A shows a schematic perspective view of a section of a fluidic microsystem as in Fig. 1. However, in this case the channel bottom 51 forms a substrate for a modification layer 55. The modification layer 55 consists, for example, of a monolayer of biological cells. Again, the movement of the particle 10 is to be detected with object detection according to the invention, as described above, which occurs here through a frame-shaped mask 20. The particle 10 is a test object, which can be a biological cell or an artificial particle with specific or nonspecific binding sites (molecules). The movement of the particle 10 is influenced by the interaction with the modification layer 55, i.e. by the occurrences of adhesion which arise.

To determine the adhesion characteristics of the particle 10 relative to the modification layer 55, i.e. to determine binding forces, binding constants, and/or the dynamics of cell adhesion, the particle is pressed with the aid of the trapping laser 60 onto the surface of the modification layer 55 while the rotating field of the electrode arrangement 40 induces oscillating rotations to the left or right. The oscillatory particle vibrations in the states 11a, 11b are detected via the mask 20 as described above. Through comparison with the movement characteristics without adhesion, information on the binding forces and similar characteristics can be obtained. Other mask shapes which are different from the frame mask 20 illustrated can also be used. Fig. 13B shows the corresponding situation in a top view.

The modification can also be formed by one single particle on the channel floor 51. This situation is illustrated in Fig. 14. A biological cell 56 is on the channel floor 51. The detection of the particle movement of the particle 10 according to the invention again occurs depending on the interaction with the cell 56. For sufficiently small particles (diameter smaller than 5 μm) the surfaces of the cells 56 can also be measured with localized resolution. There is also the possibility of connecting the locally resolved partial measurement of the interactions of the cell 56 with the particle 10 with a chemical stimulation of the attached cell 56.

Fig. 15 shows a further modification of object detection for the determination of interactions of a particle with a modification layer on the channel floor 51. The modification layer consists of multiple molecular receptors 57. The particle 10 has ligands 12. The particle rotates as described above with reference to Fig. 1. It can be determined from the particle detection whether the ligand 12 undergoes binding with the receptors 57. The particle 10 can itself be a biological cell or a cell component and can

carry a receptor on its surface depending on natural conditions.

A further application of the invention for measurement of forces in a microsystem is illustrated in Figs. 16 and 17. Analogously to Fig. 1, Fig. 16 shows a section of a microsystem with the channel bottom 51 and the lower microelectrodes 41. The particle 10 is guided to a predetermined position P having the coordinates (x_1, y_1, z_1) with the trapping laser 60 and there is subjected to the rotating fields of the electrode arrangement. The imaging unit with the mask 20 is appropriately adjusted to detect the object movement. The angular velocity of the particle 10 measured at point P has a direct relationship to the field strength at this location (the angular velocity is proportional to the square of the field strength). In this way, the electromagnetic field in the microsystem in the x, y, and z directions can be measured with the object detection according to the invention using a small test particle, in that the test particle 10 is scan-like moved to various spatial positions between the microelectrodes and subjected to a rotation measurement.

For this measurement, a mask design can also be provided with which the particle movements in the entire region between the microelectrodes can be detected. In this case, the mask 20 does not have to be displaced upon adjustment to a new point P.

A further mask design with two strip-shaped segments (detection slits) is used according to Fig. 17 for determination of particle movements in the direction of the arrow. The movement of the particle 10 in the x direction is performed with the trapping laser (not shown) or through shifting the amplitudes of the high frequency voltages on the electrodes 41a, 41b and/or 41c, 41d. Information on dielectric particle characteristics, the field strength in

the focus of the trapping laser, and the electromagnetic field strength can be derived from the deflection of the particle.

Analogously to the techniques described in figs. 15 to 17, a measurement of the field strength in the trapping laser 60 through measurement of the rotational speed of a test particle depending on the distance from the focus of the trapping laser can also be used.

Object detection according to the invention is also usable for detection of particle deformations. This is illustrated in Fig. 18. The particle 10 is deformed by adjustment of an inhomogeneous high frequency electric field on the electrodes 41a, 41b and/or 41c, 41d while it is held in free suspension with the trapping laser. The deformation can, for example, lead from a round particle shape (upper part of Fig. 18) to an elliptical particle shape (lower part of Fig. 18). With a slit mask, having two strip-shaped segments which are set up to transmit light from the sections 80a, 80b of the microsystem to the detector, the asymmetry of the particle 10 can be detected. Mechanical characteristics of the particle (e.g. biological cell) can be estimated from the deformation, which is derived from the detector signal. Depending on the application, other mask shapes which are adjusted to the respective asymmetries can also be used for examination of the deformation.

Fig. 19 is an overview illustration of a device according to the invention for object detection with implementation of the invention on a fluidic microsystem. The fluidic microsystem 110, which contains a suspension with at least one particle to be examined, is driven via a control device 111. If the microsystem contains microelectrodes for dielectric particle manipulation, then the control device 111 particularly contains a generator for driving the electrodes.

The region of interest of the microsystem 110 is imaged via optical elements 121 enlarged on the structured mask 120, which can be adjusted in relation to the microsystem with an adjustment unit 122. In an integrated manner, the light passing through the structured mask 120 is imaged on the detector 123 (e.g. photodiode) by further optical elements 121, which possibly include a stop filter for the light of the trapping laser 160. The detector 123 is connected with an evaluation unit 124 which particularly contains a computing unit for evaluating the signal traces and a display unit for visual depiction of the object characteristics detected. The evaluation of the signal traces is performed in a way known per se, particularly in regard to the temporal position of the maxima, the amplitudes of the signals, and their phase positions.

Fig. 19 further shows the trapping laser 160, which is controlled via a separate laser tweezers control 161. The reference sign 200 indicates an overall control unit for synchronous operation, depending on the application, of the laser control 161, the control unit 111, and the adjustment unit 122.

The imaging unit with the optical elements and the structured mask 120 is preferably integrated in a microscope whose features are not illustrated. The trapping laser 160 can also be directed into the microsystem 110 via the microscope.

In an alternative design of the device according to the invention, the structured masks are directly implemented on the light sensitive surface of the detector. Furthermore, it can be provided that the detector is not formed by a single photodiode, but by a CCD matrix. In this type of design, imaging of the locational area of the particle on the CCD matrix and subsequent electronic masking of the matrix

signal through evaluation of the signals from specific image points can be performed.

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CLAIMS (as originally filed and published)

1. A process for object detection, with the steps:
 - enlarged optical imaging of at least one resting or moving object (10) on a structured mask (20) with at least one segment (30) which is adapted for transmitting light from a flat section (80), in which the object (10) is located at least partially or temporarily and which has a characteristic dimension smaller than the dimension of the object (10) or its movement path, to a detector unit (123),
 - detection of the quantity of light transmitted by the structured mask (20) and generation of a detector signal which has a predetermined relationship with the quantity of light, and
 - evaluation of the detector signal in regard to the presence of the object (10), its position, its shape, and/or the temporal change of the position.
2. The process according to claim 1, wherein the object detection is performed on synthetic or biological particles (10) in a microchannel of a fluidic microsystem in which the particle is subjected to hydrodynamic, acoustic, magnetic, and/or electrical forces.
3. The process according to claim 2, wherein the mask (20) is positioned in relation to the microsystem in such a way that light is transmitted by the mask from a section (80) in which the particle (10) is to be positioned or moved.
4. The process according to claim 2, wherein the mask (20) is positioned in relation to the microsystem in such a way that light is transmitted by the mask from

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a section (80) into which the particle (10) is not to enter.

5. The process according to one of the preceding claims, wherein
 - to detect the presence of a resting particle (10), it is detected whether the detector signal (D1) has a predetermined, unchanging amplitude,
 - to detect the presence of a moving particle (10) at a specific position, it is determined whether the detector signal has a predetermined time characteristic,
 - to detect the frequency and speed of particles (10), maxima of the detector signal are evaluated in regard to their width and their interval, and/or
 - to count particles (10), the maxima of the detector signal are counted.
6. The process according to claim 5, wherein determination of the direction of the particle movement and/or size-dependent particle counting is performed.
7. The process according to one of the preceding claims, wherein the amplitude of the detector signal and/or the variability of the detector signal are evaluated.
8. The process according to one of the preceding claims 2 to 7, wherein the particle (10) is fixed or moved with a trapping laser.
9. The process according to claim 8, wherein the particle (10) is brought into contact with a modification layer (55), a cell (56), or receptors (57) in the microsystem with the trapping laser (60) and, during the evaluation of the detector signal in regard to the movement characteristics of the particle (10), parameters are determined which are characteristic for the

interaction of the particle (10) with the modification layer (55), the cell (56), or the receptors (57).

10. A device for object detection, which comprises:
 - an optical imaging unit for enlarged imaging of at least one resting or moving object (10) on a structured mask (20), having at least one light transmitting segment (30) which is set up for the purpose of transmitting light from a flat section (80), in which the object (10) is located at least partially or temporarily and which has a characteristic dimension smaller than the dimension of the object (10) or its movement path, to a detector unit (123),
 - a detector unit (123) for detecting the quantity of light transmitted by the structured mask (20) and for forming a detector signal which has a predetermined relationship with the quantity of light, and
 - an evaluation unit for evaluation of the detector signal in regard to the presence of the object (10), its position, its shape, and/or the temporal change of the position.
11. The device according to claim 10, wherein the optical imaging unit is part of a microscope.
12. The device according to claim 11, wherein the mask (20) is positioned in the beam path of the microscope.
13. The device according to one of the claims 10 to 12, wherein the mask (20) is a transmission screen with at least one transparent segment (30).
14. The device according to claim 13, wherein multiple segments are provided which are positioned two-dimensionally in the plane of the mask.

15. The device according to claim 13 or 14, wherein cross-shaped segments, frame-shaped segments, and/or straight or curved strip-shaped segments are provided.
16. The device according to one of the claims 10 to 15, wherein the detector unit (123) is set up for integrated detection of the partial image of the object (10) or its movement path transmitted or reflected by the mask (20).
17. The device according to one of the claims 10 to 16, which is set up for object detection of synthetic or natural particles (10) in a fluidic microsystem.
18. The device according to claim 17, wherein the particles (10) in the microsystem are subjected to hydrodynamic, acoustic, magnetic, and/or electrical forces.
19. The device according to claim 17 or 18, wherein a trapping laser arrangement (60, 160) is provided for manipulation of the particles (10) in the microsystem.
20. The device according to one of the claims 10 to 19, wherein the segment (30) has a characteristic dimension which is smaller than the object (10) or its movement path or is smaller than the image of the object (10) or its movement path.
21. The use of a process or device according to one of the preceding claims for
 - dielectric single particle spectroscopy in fluidic microsystems,
 - measurement of electromagnetic forces in microelectrode arrangements,
 - measurement of optical forces in trapping lasers,
 - detection of the function of microelectrodes in microsystems,

- detection of particle positions and/or movements, particle numbers, and/or particle interactions, and/or
- measurement of particle rotations which are induced by rotating electrical fields.

Table 1	
Summary of the results of the 1990-1991 survey of the health status of the population of the Republic of Serbia	
1. General characteristics of the population	
1.1. Total population	10,000,000
1.2. Urban population	6,000,000
1.3. Rural population	4,000,000
1.4. Population density	100 inhabitants/km ²
1.5. Life expectancy at birth	75 years
1.6. Infant mortality rate	10 per 1,000 live births
1.7. Fertility rate	1.5 children per woman
1.8. Sex ratio	100 males per 100 females
1.9. Age structure	
1.9.1. 0-14 years	15%
1.9.2. 15-64 years	65%
1.9.3. 65+ years	20%
2. Health status of the population	
2.1. Prevalence of chronic diseases	
2.1.1. Hypertension	25%
2.1.2. Diabetes mellitus	5%
2.1.3. Coronary artery disease	10%
2.1.4. Chronic obstructive pulmonary disease	8%
2.1.5. Rheumatoid arthritis	3%
2.1.6. Multiple sclerosis	1%
2.1.7. Other chronic diseases	5%
2.2. Prevalence of mental disorders	
2.2.1. Depression	10%
2.2.2. Anxiety disorders	5%
2.2.3. Schizophrenia	2%
2.2.4. Other mental disorders	3%
2.3. Prevalence of infectious diseases	
2.3.1. Tuberculosis	1%
2.3.2. HIV/AIDS	0.5%
2.3.3. Hepatitis B	0.2%
2.3.4. Other infectious diseases	0.3%
2.4. Prevalence of injuries and poisoning	
2.4.1. Road traffic accidents	0.5%
2.4.2. Falls	0.2%
2.4.3. Other injuries and poisoning	0.3%
2.5. Prevalence of congenital anomalies	
2.5.1. Down's syndrome	0.1%
2.5.2. Other congenital anomalies	0.1%
2.6. Prevalence of cancer	
2.6.1. Lung cancer	0.5%
2.6.2. Breast cancer	0.4%
2.6.3. Prostate cancer	0.3%
2.6.4. Other cancer	0.2%
2.7. Prevalence of dental diseases	
2.7.1. Caries	15%
2.7.2. Periodontitis	10%
2.7.3. Other dental diseases	5%
2.8. Prevalence of skin diseases	
2.8.1. Eczema	5%
2.8.2. Psoriasis	3%
2.8.3. Other skin diseases	2%
2.9. Prevalence of eye diseases	
2.9.1. Glaucoma	2%
2.9.2. Cataracts	1%
2.9.3. Other eye diseases	1%
2.10. Prevalence of ear, nose and throat diseases	
2.10.1. Otitis media	5%
2.10.2. Rhinitis	3%
2.10.3. Other ear, nose and throat diseases	2%
2.11. Prevalence of musculoskeletal diseases	
2.11.1. Osteoarthritis	10%
2.11.2. Rheumatoid arthritis	3%
2.11.3. Other musculoskeletal diseases	2%
2.12. Prevalence of neurological diseases	
2.12.1. Multiple sclerosis	1%
2.12.2. Other neurological diseases	1%
2.13. Prevalence of endocrine diseases	
2.13.1. Diabetes mellitus	5%
2.13.2. Other endocrine diseases	1%
2.14. Prevalence of reproductive system diseases	
2.14.1. Prostate cancer	0.3%
2.14.2. Other reproductive system diseases	0.2%
2.15. Prevalence of urinary system diseases	
2.15.1. Kidney stones	0.5%
2.15.2. Other urinary system diseases	0.2%
2.16. Prevalence of digestive system diseases	
2.16.1. Gastritis	5%
2.16.2. Ulcer	3%
2.16.3. Other digestive system diseases	2%
2.17. Prevalence of respiratory system diseases	
2.17.1. Chronic obstructive pulmonary disease	8%
2.17.2. Asthma	3%
2.17.3. Other respiratory system diseases	2%
2.18. Prevalence of circulatory system diseases	
2.18.1. Hypertension	25%
2.18.2. Coronary artery disease	10%
2.18.3. Other circulatory system diseases	2%
2.19. Prevalence of immune system diseases	
2.19.1. HIV/AIDS	0.5%
2.19.2. Other immune system diseases	0.2%
2.20. Prevalence of other diseases	
2.20.1. Cancer	0.5%
2.20.2. Other diseases	0.2%
2.21. Prevalence of injuries and poisoning	
2.21.1. Road traffic accidents	0.5%
2.21.2. Falls	0.2%
2.21.3. Other injuries and poisoning	0.3%
2.22. Prevalence of congenital anomalies	
2.22.1. Down's syndrome	0.1%
2.22.2. Other congenital anomalies	0.1%
2.23. Prevalence of cancer	
2.23.1. Lung cancer	0.5%
2.23.2. Breast cancer	0.4%
2.23.3. Prostate cancer	0.3%
2.23.4. Other cancer	0.2%
2.24. Prevalence of dental diseases	
2.24.1. Caries	15%
2.24.2. Periodontitis	10%
2.24.3. Other dental diseases	5%
2.25. Prevalence of skin diseases	
2.25.1. Eczema	5%
2.25.2. Psoriasis	3%
2.25.3. Other skin diseases	2%
2.26. Prevalence of eye diseases	
2.26.1. Glaucoma	2%
2.26.2. Cataracts	1%
2.26.3. Other eye diseases	1%
2.27. Prevalence of ear, nose and throat diseases	
2.27.1. Otitis media	5%
2.27.2. Rhinitis	3%
2.27.3. Other ear, nose and throat diseases	2%
2.28. Prevalence of musculoskeletal diseases	
2.28.1. Osteoarthritis	10%
2.28.2. Rheumatoid arthritis	3%
2.28.3. Other musculoskeletal diseases	2%
2.29. Prevalence of neurological diseases	
2.29.1. Multiple sclerosis	1%
2.29.2. Other neurological diseases	1%
2.30. Prevalence of endocrine diseases	
2.30.1. Diabetes mellitus	5%
2.30.2. Other endocrine diseases	1%

DECLARATION FOR PATENT APPLICATION

Docket Number (optional) B1180/20003
Sheet 1 of 2

I, as a below named inventor, I hereby declare that:

My residence, post office address and citizenship are as stated below next to my name.

I believe I am the original, first and sole inventor (if only one name is listed below) or an original, first and joint inventor (if plural names are listed below) of the subject matter which is claimed and for which a patent is sought on the invention entitled:

PROCESS AND DEVICE FOR THE DETECTION OF MICROSCOPICALLY SMALL OBJECTS

The specification of which is attached hereto unless the following box is checked:

Was filed on January 26, 2000 as United States Application Number or PCT International Application
Number PCT/EP00/00621 and was amended on _____ (if applicable).

I hereby state that I have reviewed and understand the contents of the above identified specification, including the claims, as amended by any amendment referred to above. I acknowledge the duty to disclose information which is material to patentability as defined in 37 CFR §1.56. I hereby claim foreign priority benefits under 35 U.S.C. §119 (a)-(d) or §365(b) of any foreign application(s) for patent or inventor's certificate, or §365 (a) of any PCT International application which designated at least one country other than the United States, listed below and have also identified below, by checking the box, any foreign application for patent or inventor's certificate, or PCT International application having a filing date before that of the application on which priority is claimed.

Prior Foreign Application(s)

Priority Claimed

<u>99 03 001.4</u>	<u>Germany</u>	<u>26 January 1999</u>	<u>X</u> Yes <u> </u> No
(Number)	(Country)	(Day/Month/Year Filed)	
<u> </u>	<u> </u>	<u> </u>	<u> </u> Yes <u> </u> No
(Number)	(Country)	(Day/Month/Year Filed)	

I hereby claim the benefit under 35 U.S.C. §119(e) of any United States provisional application(s) listed below.

<u> </u>	<u> </u>
(Application Number)	(Filing Date)
<u> </u>	<u> </u>
(Application Number)	(Filing Date)

I hereby claim the benefit under 35 U.S.C. § 120 of any United States application(s) or § 365(c) of any PCT International application designating the United States, listed below and, insofar as the subject matter of each of the claims of this application is not disclosed in the prior United States or PCT International application in the manner provided by the first paragraph of 35 U.S.C. § 112, I acknowledge the duty to disclose information which is material to patentability as defined in 37 CFR §1.56 which became available between the filing date of the prior application and the national or PCT International filing date of this application.

<u>PCT/EP00/00621</u>	<u>26 January 2000</u>	<u>pending</u>
(Application Number)	(Filing Date)	(Status-patented, pending, abandoned)
<u> </u>	<u> </u>	<u> </u>
(Application Number)	(Filing Date)	(Status-patented, pending, abandoned)

I hereby appoint the following attorney(s) and/or agent(s) to prosecute this application and to transact all business in the Patent and Trademark Office connected therewith:

Alan H. Bernstein (Registration No. 19,315); Stanley H. Cohen (Registration No. 20,235); Manny D. Pokotilow (Registration No. 22,492); Barry A. Stein (Registration No. 25,257); Martin L. Faigus (Registration No. 24,364); Eric S. Marzluf (Registration No. 27,454); Robert S. Silver (Registration No. 35,681); Scott Slomowitz (Registration No. 39,032); Michael J. Berkowitz (Registration No. 39,607); David M. Tener (Registration No. 37,054); James J. Kozuch (Registration No. 39,733); Frank M. Linguiti (Registration No. 32,424); Gary A. Greene (Registration No. 38,897); Michael J. Cornelison (Registration No. 40,395); Christopher Carrone (Registration No. 46,101); and Allan H. Fried (Registration No. 31,253), care of Caesar, Rivise, Bernstein, Cohen & Pokotilow, Ltd., 12th Floor, Seven Penn Center, 1635 Market Street, Philadelphia, Pennsylvania 19103-2212, my attorneys with full power of substitution and revocation, to prosecute this application and transact all business in the Patent and Trademark Office connected therewith.

I hereby declare that all statements made herein of my own knowledge are true and that all statements made on information and belief are believed to be true; and further that these statements were made with the knowledge that willful false statements and the like so made are punishable by fine or imprisonment, or both, under Section 1001 of Title 18 of the United States Code and that such willful false statements may jeopardize the validity of the application or any patent issued hereon.

Full name of sole or first inventor (given name, family name) GÜNTHER FUHRInventor's signature Günter Fuhr Date 20/08/01Residence Berlin, Germany Citizenship GermanPost Office Address Kavalierstrasse 15, D-13187 Berlin, GermanyFull name of second joint inventor, if any (given name, family name) THOMAS SCHNELLESecond Inventor's signature Thomas Schnell Date 3.9.01Residence Berlin, Germany Citizenship GermanPost Office Address Koppenstrasse 65, D-10243 Berlin, Germany

Additional inventors are being named on separately numbered sheets attached hereto.

DECLARATION FOR PATENT APPLICATION

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Inventor's signature _____ Date _____

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Second Inventor's signature H. Glasser Date 22.08.2001

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DECLARATION FOR PATENT APPLICATION

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